

1 **Recovery of Neurophysiological Measures in Post-COVID Fatigue – a**
2 **12-month Longitudinal Follow-up Study**

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8

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Abstract

10 One of the major consequences of the COVID-19 pandemic has been the significant incidence of
11 persistent fatigue following resolution of an acute infection (i.e. post-COVID fatigue). We have
12 shown previously that, in comparison to healthy controls, those suffering from post-COVID fatigue
13 exhibit changes in muscle physiology, cortical circuitry, and autonomic function. Whether these
14 changes preceded infection, potentially predisposing people to developing post-COVID fatigue, or
15 whether the changes were a consequence of infection was unclear. Here we present results of a 12-
16 month longitudinal study of 18 participants from the same cohort of post-COVID fatigue sufferers to
17 investigate these correlates of fatigue over time. We report improvements in self-perception of fatigue
18 via questionnaires, as well as significant improvements in objective measures of peripheral muscle
19 fatigue and autonomic function, bringing them closer to healthy controls. Additionally, we found
20 reductions in muscle twitch tension rise times, becoming faster than controls, suggesting that the
21 improvement in muscle fatigability might be due to a process of adaptation rather than simply a return
22 to baseline function.

23

Introduction

24

25 In May 2023, more than three years into the pandemic, the World Health Organization (WHO)
26 Emergency Committee on COVID-19 recommended that the pandemic no longer represented a public
27 health emergency of international concern¹. However, while acute COVID-19 may no longer
28 constitute a global emergency, the long-term effects of severe acute respiratory syndrome coronavirus
29 2 (SARS-CoV-2) infection are now becoming apparent. Although the majority of infected individuals
30 experience mild symptoms or recover within a few weeks, a significant proportion continue to
31 experience persistent symptoms beyond the acute phase²⁻⁴, a condition commonly known as long
32 COVID or post-acute sequelae of SARS-CoV-2 infection.

33 Long COVID is characterized by a diverse range of symptoms, including fatigue, cognitive
34 impairment, respiratory issues, and musculoskeletal problems⁵⁻⁷. Among these, muscle pathology has
35 emerged as a common and debilitating feature, even in individuals with a history of mild COVID-
36 19⁸. Reports highlight muscle weakness, myalgia, and impaired motor coordination among long
37 COVID patients^{2,5,9}, significantly impacting their quality of life and functional abilities.

38 Physiological muscle stimulation during physical activity leads to the production of myokines, which
39 normally induce an anti-inflammatory environment. However, in the presence of the SARS-CoV-2
40 virus, myokine production instead stimulates a prolonged muscular inflammatory environment^{10,11}.
41 Inflammation impairs muscle protein synthesis and mitochondrial activity, and thus has the potential
42 to induce long-term sarcopenia¹².

43 To form a comprehensive understanding of the mechanisms underlying long COVID, longitudinal
44 studies are crucial. These allow the evaluation of clinical, immunological, radiological and
45 neurophysiological changes over time, providing insights into the patterns of recovery of these
46 metrics. Comparison of recovery time courses between clinical measures and biomarkers could
47 potentially address whether abnormal measures play a causal role in the disease, or are simply
48 correlated with its downstream consequences.

49 In a previous study¹³ we demonstrated changes in muscle physiology in long COVID after non-severe
50 SARS-CoV-2 infection, where there had been no requirement for acute hospital in-patient care. These
51 changes might explain some of the symptoms of fatigue described by patients. Here we report a
52 longitudinal follow-up study in a subset of the same cohort, in whom neurophysiological
53 measurements and subjective perception of fatigue were repeated twice more, at 6 month intervals.
54 Levels of fatigue improved significantly after a year; for most of the neurophysiological metrics there
55 was likewise a return to levels seen in age and sex-matched controls. We therefore suggest that these
56 changes in muscle physiology and autonomic function occur as a consequence of a SARS-CoV-2

57 infection, rather than a pre-existing phenotype that increased susceptibility to developing post-
58 COVID fatigue.

59 **Methods**

60 Our previous publication¹³ employed 35 non-invasive behavioural and neurophysiological tests to
61 assess specific circuits within the central, peripheral and autonomic nervous systems. In this
62 longitudinal follow up study, we used only the sub-set of these tests which were significantly different
63 between people with pCF and controls in our original paper. Transcranial Magnetic Stimulation
64 (TMS) allowed us to probe the state of cortical motor circuits. Electrical stimulation of muscles
65 assessed peripheral fatigue, recordings of heart rate assessed the state of the autonomic nervous
66 system, and blood oxygen saturation (SaO₂) was also collected. Participants completed a fatigue
67 impact scale (FIS) questionnaire via a web-based survey tool.

68 **Participants**

69 The study was approved by the Ethics Committee of Newcastle University Faculty of Medical
70 Sciences; participants provided written informed consent.

71 Measures collected in our initial study¹³ were used here as baseline data. This included data from a
72 cohort of 37 participants (27 female) who were suffering from pCF by self-report and a second cohort
73 of 52 volunteer controls (37 female) with no symptoms of fatigue. Inclusion criteria were age 18–65
74 years, with no history of neurological disease. The first visit to the laboratory was made 6–26 weeks
75 after infection for the pCF cohort. In the control cohort, six subjects had reported having mild
76 COVID-19 but with complete recovery and no symptoms of pCF. Of the 37 people with pCF, 18
77 participated in this longitudinal follow-up study (13 female), completing a further two lab visits at
78 intervals of approximately 6 months to yield a total of three visits.

79 **General Electrophysiological Methods**

80 Electromyographic activity (EMG) was recorded with adhesive surface electrodes positioned over
81 muscles (Kendall H59P, Covidien, Dublin, Ireland) using an isolated amplifier (D360, Digitimer,
82 Welwyn Garden City, UK; gain 500, bandpass 30 Hz-2 kHz). Transcranial magnetic brain stimulation
83 (TMS) was given with a Bistim 200² stimulator and figure-of-eight coil (7 cm diameter for each
84 winding; Magstim Company Limited, Whitland, UK), with the coil held tangential to the head at
85 around 45° to the parasagittal plane, inducing current in the brain from posterior to anterior. Coil
86 position relative to the head was maintained using a Brainsight neuronavigation system (Brainsight,
87 Cardiff, UK). Stimulus timing was controlled by a Power1401 intelligent laboratory interface running
88 Spike2 software (Cambridge Electronic Design, Cambridge, UK), which also sampled EMG and

89 other task-related signals to hard disk (sampling rate 5 kSamples/s). All measurements were made on
90 the self-reported dominant side. Offline analysis was performed with custom scripts written in the
91 MATLAB programming environment.

92 **Paired-Pulse TMS**

93 EMG was recorded from the first-dorsal interosseous (1DI); the TMS coil was moved to locate the
94 hot spot for this muscle. The resting motor threshold (RMT) was determined, as the intensity required
95 to generate MEPs of amplitude greater than 100 μ V on 3/6 sweeps. The test stimulus intensity was
96 set to generate MEP amplitudes of 1 mV, or to 1.2xRMT, whichever was lower. The conditioning
97 stimulus intensity was 0.8xRMT. We then measured the responses to the test stimulus alone, and
98 when preceded by the conditioning stimulus at intervals of 10 ms, corresponding to intracortical
99 facilitation (ICF) (see Baker et al., 2023 Supplementary Figure 1). Twenty repetitions of each
100 condition were given, in pseudo-random order, with the subject at rest. Offline analysis measured the
101 peak-to-peak amplitude of responses to conditioned stimuli as a percentage of the responses to test
102 stimulus alone, yielding the measure *TMS_ICF*.

103 **Heart Rate**

104 A single channel electrocardiogram (ECG) recording was made, using a differential recording from
105 either left shoulder and right leg, or left and right shoulders (bandpass 0.3-30 Hz, gain 500, sampling
106 rate 1 kSamples/s). The ECG was processed offline to extract the time of each QRS complex and
107 compute the mean heart rate (measure *Mean_HR*). Heart rate measures were made during a Stop
108 Signal Reaction Time test, which ensured that the subject was sitting quietly, while engaged in a
109 consistent behaviour.

110 **Measures of Muscle Physiology**

111 The twitch interpolation procedure allows assessment of an individual's ability to activate a muscle
112 maximally voluntarily; in this study, we also measured changes after a sustained (fatiguing)
113 contraction¹⁴. The protocol followed previous work from this laboratory¹⁵ and was identical to that
114 used in Baker, et al.¹³. Subjects sat with their dominant arm and forearm strapped into a dynamometer
115 to measure torque about the elbow; the shoulder was flexed, and the elbow at a right angle, so that
116 the upper arm was horizontal and the forearm vertical. The forearm was supinated. Thin stainless-
117 steel plate electrodes (size 30x15 mm) were wrapped in saline-soaked cotton gauze and taped over
118 the belly of the biceps muscle (cathode) and its distal tendon (anode). Electrical stimuli were delivered
119 through these electrodes while monitoring the evoked twitch response recorded by the dynamometer,
120 and the intensity increased until the response grew no further. This supramaximal stimulus was used
121 for all subsequent measurements.

122 The following recordings were then made in sequence; this protocol was followed to maintain
123 consistency with our original study. A brief tone cued the subject to produce and hold a maximal
124 voluntary contraction; 2 s after the tone, a stimulus was given to the biceps, and 1 s later a second
125 tone indicated that the subject should relax. Five seconds later, a biceps stimulus was given, followed
126 by a further 55 s rest period. This sequence was repeated three times. A long tone then cued the
127 subject to make a sustained maximal voluntary contraction. This was continued either for 90 s, or
128 until the force exerted fell to 60% of the initial maximal level. During this sustained contraction, the
129 biceps was stimulated every 10 s. After the contraction ended, a final three biceps stimuli were given
130 at rest (inter-stimulus interval 5 s).

131 From the three stimuli delivered at rest at the start, we averaged the maximal twitch at rest and
132 measured its amplitude, F_{rest}^{before} . From the three stimuli delivered at rest after the sustained
133 contraction, we measured F_{rest}^{after} .

134 Peripheral fatigue (measure $TI_PeriphFatigue$) was calculated as:

135
$$TI_PeriphFatigue = \frac{F_{rest}^{after}}{F_{rest}^{before}} 100\%$$

136 This describes the reduced ability of the muscle to generate force after fatigue, even when activation
137 is performed independent of the central nervous system by an electrical stimulus to the muscle.
138 Additionally, we measured the time to maximal force generation following direct electrical
139 stimulation to the muscle (measure *Rise Time*) using the twitch initially evoked at rest.

140 **Biometric Data**

141 Blood oxygen saturation was measured using a pulse oximeter placed onto the index finger (SaO_2).

142 **Statistics**

143 Descriptive statistics are given as mean \pm standard deviation (SD). Comparisons for each metric
144 across visits were carried out using a repeated measures ANOVA (using the 'fitrm' function in
145 MATLAB). Correlation between measures was assessed with linear regression and results reported
146 as r^2 values. Paired t-tests were used to compare individual measures between visits. Unpaired t-tests
147 were used to compare measures between different cohorts.

148

Results

149 Figure 1A shows the time line of the repeat visits of the 18 participants (13 females; age 48.1 ± 10.0
150 years) for whom we collected longitudinal data. Visits 2 (V2) and 3 (V3) were on average 6.02 ± 0.34
151 and 11.61 ± 0.36 months after visit 1 (V1).

152 **Fatigue Impact Scale**

153 There was a significant ($p < 0.0001$, $F = 13.3$) decrease in the self-reported perception of fatigue across
154 visits; mean FIS score declined from 80.3 at V1 to 60.2 at V2 and 46.1 at V3 (Figure 1B). A similar
155 trend was seen for all of the sub-domains of the FIS score: there was a significant average decrease
156 over time in the cognitive FIS score (by 6.8 from V1 to V3, $p = 0.009$, $F = 5.5$), the social FIS score
157 (decrease 16.9, $p < 0.0001$, $F = 14.00$) and the physical FIS score (decrease 10.5, $p < 0.0001$, $F = 19.14$).
158 Overall, the majority (16/18) of participants had improved FIS scores between V1 and V3.

159 **Changes in Biological Measures**

160 Our earlier work showed that only a small number of measures (*TI_PeriphFatigue*, *TMS_ICF*,
161 *Mean_HR*, *SaO₂*) out of an extensive initial set were significantly different between controls and
162 participants suffering from pCF. Only these measures were therefore repeated during V2 and V3
163 (Figure 2). Over time there was a significant change in peripheral oxygen saturation (*SaO₂*, $p = 0.022$,
164 $F = 4.74$), heart rate (*Mean_HR*, $p = 0.033$, $F = 3.88$), and peripheral fatigue (*TI_PeriphFatigue*,
165 $p = 0.006$, $F = 6.1$). Using TMS to investigate the excitability of the primary motor cortex, we found
166 that although intracortical facilitation became more similar to controls with each visit, this trend did
167 not reach significance (*TMS_ICF*, $p = 0.075$, $F = 2.79$).

168 Post hoc comparisons showed that *SaO₂* at V2 and V3 significantly increased from V1 ($+0.71\%$,
169 $p = 0.023$ and $+1.04\%$, $p = 0.015$ respectively) but was not significantly different between V2 and V3.
170 Similarly, *mean_HR* at V2 and V3 significantly decreased relative to V1 (-4.63 bpm, $p = 0.024$ and $-$
171 5.78 bpm, $p = 0.035$ respectively). *Mean_HR* was not significantly different between V2 and V3.

172 Peripheral fatigue (*TI_PeriphFatigue*) also showed significant improvements over time. At both V2
173 and V3, *TI_PeriphFatigue* significantly increased (indicating less peripheral fatigue) compared to V1
174 ($+17.49\%$, $p = 0.01$ and $+18.02\%$, $p = 0.008$ respectively), but values at V3 were not significantly
175 different from those at V2.

176 Although both FIS scores and the biological metrics improved significantly over the course of the 12
177 month study, surprisingly there was no significant correlation between change in FIS scores and
178 changes in any of these measures (r^2 values: *TMS_ICF* 0.00063, *SaO₂* 0.011, *Mean_HR* 0.17,
179 *TI_PeriphFatigue* 0.086, all p -values > 0.05).

180 **Additional Measures of Muscle Physiology**

181 To investigate the potential mechanisms underlying improvements seen with peripheral fatigue over
182 time, we made one further measure of muscle physiology - the rise time of a maximal twitch
183 (*RiseTime*). This refers to the time taken from direct muscle stimulation to the peak force generated
184 (measured from the biceps, at rest at the start of the twitch interpolation protocol; Figure 3A).
185 Although, relative to controls, there was no significant difference at V1 ($p=0.734$), *RiseTime* did
186 become significantly different from controls at both V2 ($p=0.012$) and V3 ($p=0.002$). Furthermore,
187 *RiseTime* of the pCF cohort significantly changed over time ($p<0.0001$, $F= 19.94$). Post hoc
188 comparisons showed that at both V2 and V3, *RiseTime* significantly decreased relative to V1 (-9.8
189 ms, $p<0.001$ and -11.8 ms, $p<0.001$ respectively). *RiseTime* was not significantly different between
190 V2 and V3.

191 **Discussion**

192 A substantial proportion of people in the UK (2.9%) continue to suffer from longer-term sequelae of
193 SARS-COV-2 infection (Long COVID)¹⁶. Of various lingering symptoms such as difficulty
194 concentrating (51%), muscle aches (49%) and shortness of breath (48%), persistent fatigue is one of
195 the most common (72%)¹⁶. Persistent fatigue after a (non-SARS-CoV-2) viral infection is well known
196 to the clinician but is also a hallmark of several autoimmune and neurological disorders, suggesting
197 a link with nervous system dysfunction. Recent work has shown that even a mild to moderate COVID-
198 19 infection can cause dysregulation in the nervous system¹⁷.

199 In our previous study¹³, we provided evidence that measures of the central (intracortical facilitation,
200 *TMS_ICF*), peripheral (peripheral fatigue, *TI_PeriphFatigue*) and autonomic (mean heart rate,
201 *Mean_HR* and peripheral oxygen saturation, *SaO₂*) nervous systems were different between people
202 with pCF compared to sex- and age-matched controls. However, these findings could not infer
203 causation; measures could have been different prior to the infection (and thus conferred an increased
204 likelihood of developing pCF) or the abnormal measures could be a consequence of the infection (and
205 hence might be useful as a biomarker for tracking changes in fatigue). To address this, we repeated
206 measurements 6 months and 12 months later. As a group the reported levels of fatigue improved, and
207 our metrics returned to or were returning to normal. This suggests that the changes were mediated by
208 SARS-CoV-2 infection, rather than being a pre-existing long-term trait amongst the pCF sufferers.

209 The most significant change over time was observed in muscle fatigue. *TI_PeriphFatigue* increased
210 from 37% at the first lab visit to 55% one year later, indicating that muscles undergo significant
211 physiological changes during recovery. Acute SARS-COV-2 infection can affect skeletal muscle
212 through several mechanisms. Firstly, the virus can cause direct muscle cell damage by entering host

213 cells via the ACE-2 receptor and TMPRSS2 protein¹⁸, both of which are expressed by
214 musculoskeletal tissue¹⁹. In muscle, there is some evidence that SARS-CoV-2 may impair
215 mitochondrial function directly causing critical illness myopathy²⁰. Secondly, patients can develop
216 acute respiratory distress syndrome^{21,22}, characterised by severe hypoxaemia, thereby diminishing
217 systemic oxygen supply to muscle tissue. Hypoxia significantly affects mitochondrial activity,
218 compromising muscle energy generation needed for protein synthesis and muscle contraction^{23,24}.
219 Thirdly, SARS-COV-2 infection can cause a hyper-inflammatory state in muscle^{10,11}. Inflammation,
220 similar to hypoxia, also impairs mitochondrial function²⁵.

221 Aside from the potential direct actions of SARS-CoV-2 on mitochondria (see above), there may also
222 be indirect effects of SARS-COV-2 on mitochondrial function that contribute to ongoing fatigue
223 encountered in long COVID. For example, there is evidence in critical illness that mitochondrial
224 haplotype conveys survival advantage²⁶. In sepsis, mitochondrial dysfunction results in
225 diaphragmatic myopathy²⁷, and the extent of mitochondrial DNA depletion, measurable in
226 mononuclear cells, correlates with the severity of critical illness²⁸. It is thus possible that those who
227 develop pCF might have subclinical mitochondrial dysfunction, subsequently unmasked by SARS-
228 COV-2 infection, leaving them with systemically impaired mitochondrial function, as is typical of
229 the pattern in mitochondrial disease²⁹, potentially explaining the broad spectrum of symptoms
230 experienced by patients suffering from long COVID.

231 Whilst sepsis-related multi-system mitochondrial dysfunction may play a role in the pathophysiology
232 of long COVID, there is clear evidence for a specific role of mitochondrial dysfunction in critical
233 illness myopathy^{30,31}. Presumably this is a result of metabolic adaptations, including a shift away
234 from energy generation in mitochondria through oxidative phosphorylation and towards anaerobic
235 glycolysis, where pyruvate is converted into lactate³², an excess of which favours the maintenance of
236 inflammatory processes³³.

237 Our cohort with pCF showed significantly less peripheral fatigue 6 months and 12 months after they
238 were first assessed. Interestingly, as the pCF cohort recovered from the symptoms of fatigue, their
239 twitch tension rise times became faster than controls (Figure 3B). This suggests that the improvement
240 in fatigability of muscles over time might be due partly to a process of adaptation rather than a
241 complete return to baseline physiology. We do not know whether rise time would eventually return
242 to baseline values over a time course of more than the one year interval in our study.

243 Persistent muscle pathology, initiated in the acute phase of the disease and perhaps best explained by
244 mitochondrial dysfunction, could lead to dysfunction in type 1 muscle fibres. Although this is
245 speculation, it would theoretically result in an adaptive over dependence on type 2 fibres for force

246 generation, with faster muscle contractions but more rapid fatigue. A similar change in fibre type is
247 recognized in mitochondrial myopathy, where histopathology is reported to show an increased ratio
248 of type 2 to type 1 fibres³⁴. More recently, proteins involved in mitochondrial fusion/fission have
249 been implicated in the intracellular signalling processes regulating fibre type switching³⁵, as observed
250 in response to exercise³⁶.

251 Although our biological metrics returned to levels that were compatible with controls and reported
252 reduced levels of fatigue (Figure 1B), we found no significant correlation between changes in these
253 two. This is perhaps not surprising. While chronic fatigue will place similar limitations on all, how a
254 sufferer copes with this - and thus assesses the impact on their life - will also be affected by
255 psychological factors such as level of resilience or access to support systems. The magnitude of
256 change in FIS score, measured by a subjective questionnaire, is likely to be influenced at least as
257 much by these factors as the underlying pathology. Our findings have significant, but indirect, clinical
258 implications. Understanding the trajectory of neurophysiological recovery in long COVID has the
259 potential to inform personalized treatment approaches and rehabilitation strategies. In particular, the
260 measurement of peripheral fatigue is simple and can be achieved with low-cost equipment. This could
261 deliver an objective assessment, to be interpreted alongside subjective measures such as the FIS score.

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268 **Competing Interests**

269 The authors report no competing interests.

270 **Author Contributions**

271 DSS, MRB, and SNB designed the study. NJM and AMEB collected the data. NJM processed the
272 data. NJM, DSS, and MG performed analyses. NJM and MG wrote the manuscript. All authors
273 edited and approved the final manuscript.

274 **Data Availability Statement**

275 A spreadsheet containing values for all subject measurements across visits is available in
276 Supplementary Material.

277

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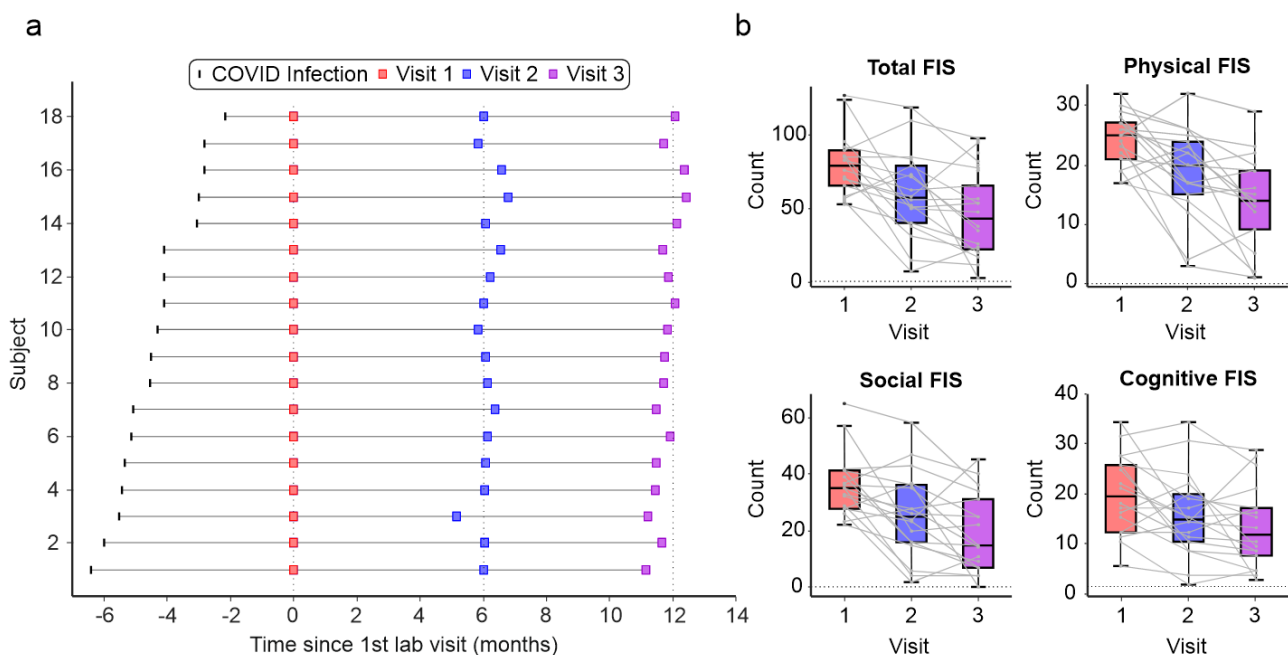
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Figure Legends

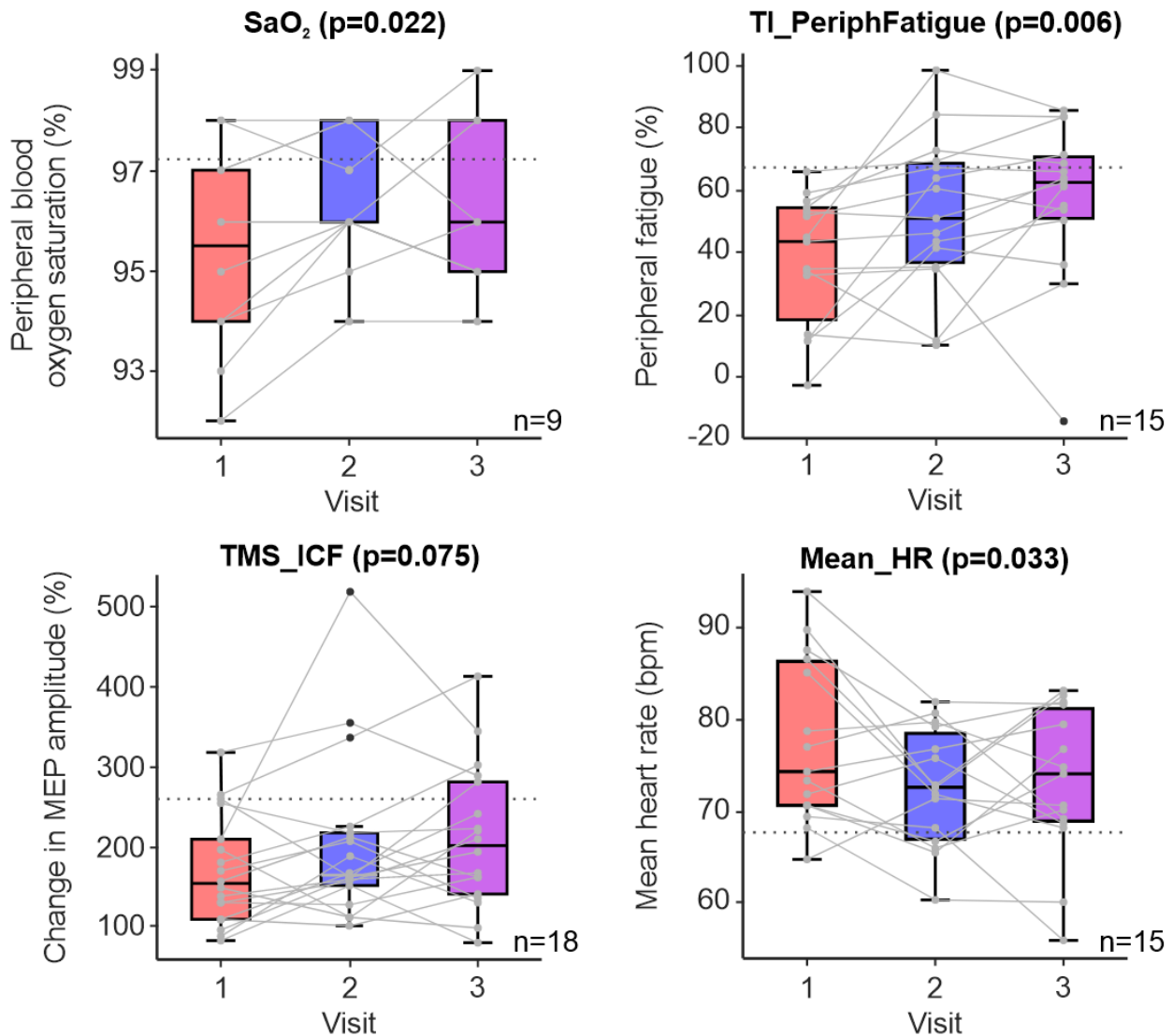


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367 **Figure 1. Timeline of visits and FIS scores.** a) Timeline of SARS-CoV-2 infection and subsequent
368 visits to the lab for assessment for each participant. b) Averaged FIS scores as box plots across all 18
369 participants for all visits; grey lines indicate individual subjects. Total FIS maximum count = 160;
370 Physical = 40; Cognitive = 40; Social = 80.

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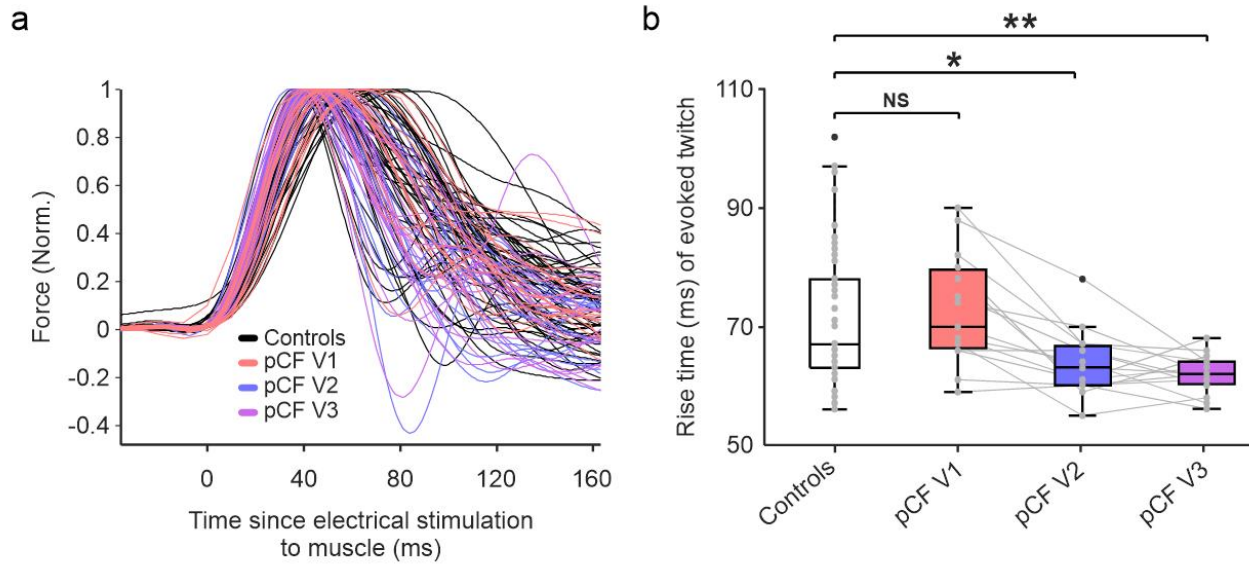


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374 **Figure 2. Changes in metrics over time.** Box plot illustration of each metric (*SaO₂*,
375 *TI_PeriphFatigue*, *TMS_ICF*, *Mean_HR*) over time. The mean of the control cohort for each metric
376 is illustrated by grey dotted lines. P values above each plot are taken from repeated measure ANOVAs
377 for each metric.

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381 **Figure 3. Rise Time.** a) Raw traces of twitch responses to direct electrical stimulation of biceps for
382 each participant, for all cohorts. The trace for each participant was normalised to the maximal force
383 generated by each individual. *RiseTime* is calculated as time from electrical stimulation to maximal
384 force generated. b) Box plots showing *RiseTime* data for controls (n=51) and post-COVID fatigue
385 participants (n=15) for each visit. NS, not significant; * P<0.05; ** P<0.005.

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